# Richardson–Lucy Algorithm Based Image Reconstruction for Proton CT

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# Imaging with protons

Páciens



### Image Reconstruction – a Huge Linear Problem

Huge linear problem:

$$\mathbf{y} \;=\; \mathbf{A} \; \mathbf{x} \;,$$

where:

- y is the energy loss of protons ⇔ track integral of RSP
- x RSP value of voxels
- A proton voxel interaction coefficients

Goal: Solve the linear problem

$$\mathbf{x} = \mathbf{f} (\mathbf{y}, \mathbf{A}).$$



#### Irradiation with protons



### Stopping Power



#### Relative Stopping Power



### Motivation and role of proton imaging

- Nowadays the importance of the proton therapy is increasing
  ⇒ more and more motivation to improve the technology
- The use of proton CT images is a promising direction
  - $\Rightarrow$  lower inaccuracy in RSP measurement
  - $\Rightarrow$  decreased safety zone around the tumour
- A pCT image measures the relative stopping power (RSP) distribution of the patient



# Bergen pCT collaboration

- Goal: reach the clinical research with a pCT prototype
- Apply monolithic active pixel sensors (MAPS)
- Use pencil beam for imaging
- Measure  $10^6$  proton / second
- Reach < 1 % RSP error



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#### Image reconstruction – Richardson – Lucy algorithm

- Originally introduced for astrophysics application
- It is a fixed point iteration for large and sparse linear problems
- Initialization: arbitrary positive vector
- Init: unit vector or precalculated approximate solution

The formula for the  $i^{th}$  element of the next image vector:

$$x_{i}^{k+1} = x_{i}^{k} \frac{1}{\sum_{j} A_{i,j}} \sum_{j} \frac{y_{j}}{\sum_{l} A_{l,j} x_{l}^{k}} A_{i,j} ,$$

where k is the number of iteration. 20-300 iteration is typical.

### Avoid the multiply calculations

Calculated for every voxel in every iteration:

$$x_i^{k+1} = x_i^k \frac{1}{\sum_j A(i,j)} \sum_j \frac{y_j}{\sum_i A(i,j) x_i^k} A(i,j) \implies x_i^{k+1} = x_i^k N_i \sum_j H_j^k A(i,j)$$
  
Calculated for every proton in every iteration:

 $H_i^k$  is called Hadamard ratio in the  $k^{\text{th}}$  iteration and defined as:

$$H_j^k = \frac{y_j}{\sum\limits_l A(l,j) x_l^k} \tag{1}$$

**Calculated for every voxel only once:**  $N_i$  is the normalization of the  $i^{\text{th}}$  voxel:

$$N_i = \frac{1}{\sum_j A(i,j)} \tag{2}$$

# GPU algorithm

#### Algorithm 1 GPU algorithm

- 1: GPU: calculate voxel normalization
- 2: for needed number of iterations do
- 3: while end of proton histories do
- 4: **CPU:** read certain amount of proton histories
- 5: **GPU:** calculate Hadamard ratio:
  - parallel calculation of proton histories
  - serial calculation of voxel interactions
- 6: **GPU:** calculate voxel contribution
  - serial calculation of proton histories
  - parallel calculation of voxel interactions
- 7: **GPU:** Update the image vector
- 8: end while
- 9: end for
- 10: CPU: Save the image vector

# Ideal imaging



# Shepp-Logan phantom – convergence without uncertainties

- Reconstructed Shepp-Logan phantom and the convergence
- The algorithm converges slower with wider uncertainty distribution



# Realistic imaging

# The incoming and outgoing pron path includes measurement uncertainties



#### Probability Density Based Proton - Voxel Interaction



#### Derenzo Phantom – Spatial Resolution

- Reconstructed RSP distribution and valley-to-peak distribution
- Spatial resolution: modulation transfer function at 10%
- My algorithm: 2.1  $\frac{lp}{cm}$  < Proton CT literature: 3.2  $\frac{lp}{cm}$



#### CTP404 Phantom – RSP Accuracy

- Reconstructed RSP distribution and avg. RSP of the inserts
- RSP accuracy: my algorithm:  $0.5\% \sim pCT$  literature: 0.4%



# Summary

#### Goal:

• Apply the Richardson-Lucy algorithm for proton CT image reconstruction

#### **Results:**

- RSP accuracy such as state of the art results in the literature
- The spatial resolution remains the week point of this algorithm
   ⇒ Requires further investigations and revisit of the simplified
   probability density based interaction calculation



# Thank you for your attention!



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