



Image reconstruction in proton computed tomography

Theory and Experiment
in High Energy Physics

Supervisors:
Gábor Bíró, Ph.D.
Gábor Papp, Ph.D.



HUN-REN
Hungarian Research Network



Zsófia Jólesz
GPU Day 2024

EÖTVÖS LORÁND
UNIVERSITY | BUDAPEST

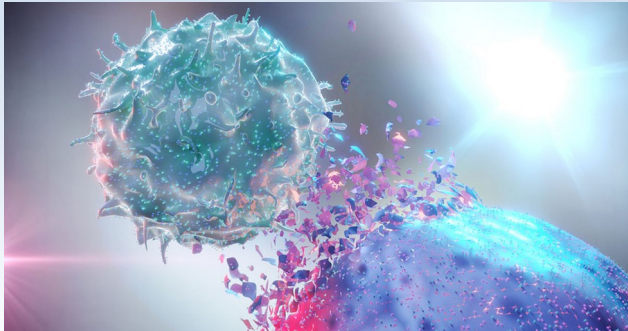
Outline

- Proton therapy – advantages and difficulties
- The Bergen Proton CT Collaboration
- Image reconstruction techniques
- Iterative methods
- The Richardson-Lucy algorithm
- Development of the framework
- Testing the algorithm with phantoms, results
- Summary

Motivation

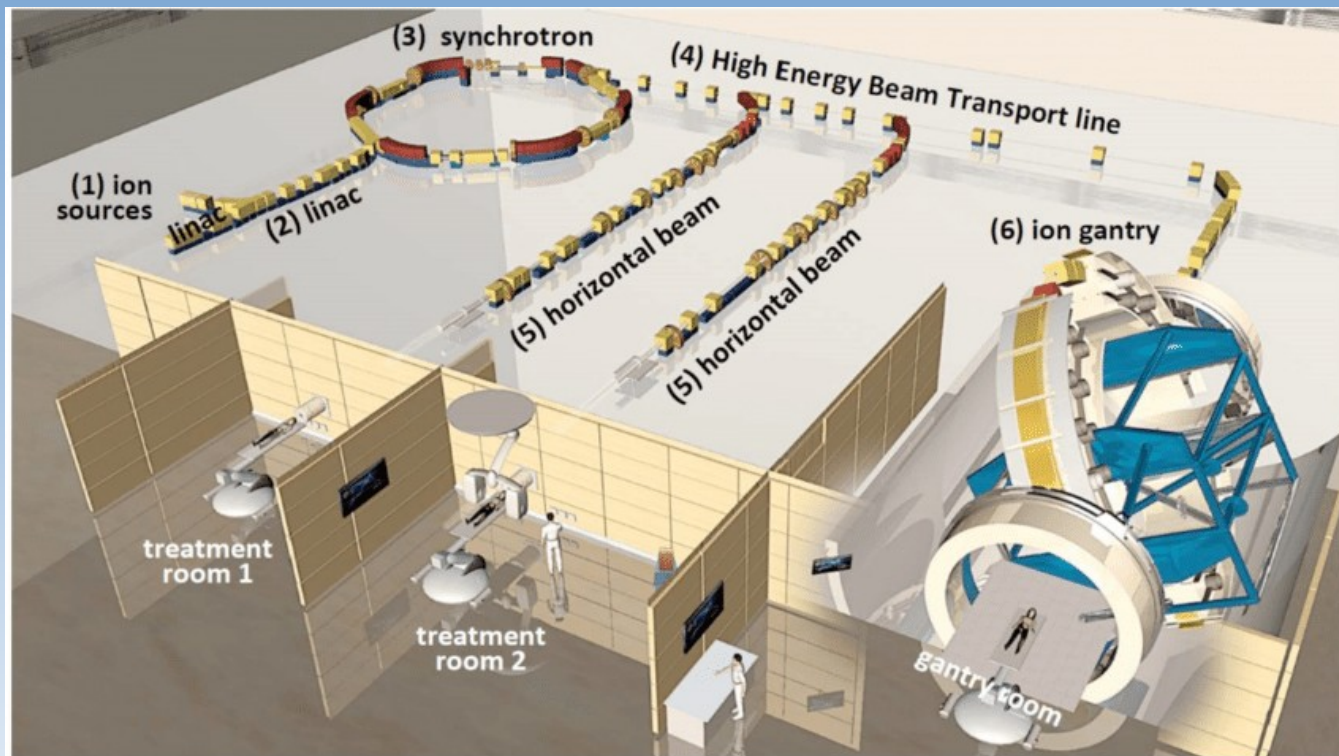


- Cancer treatment: surgery, chemotherapy, radiotherapy, immunotherapy
- Radiotherapy: uses ionizing particles



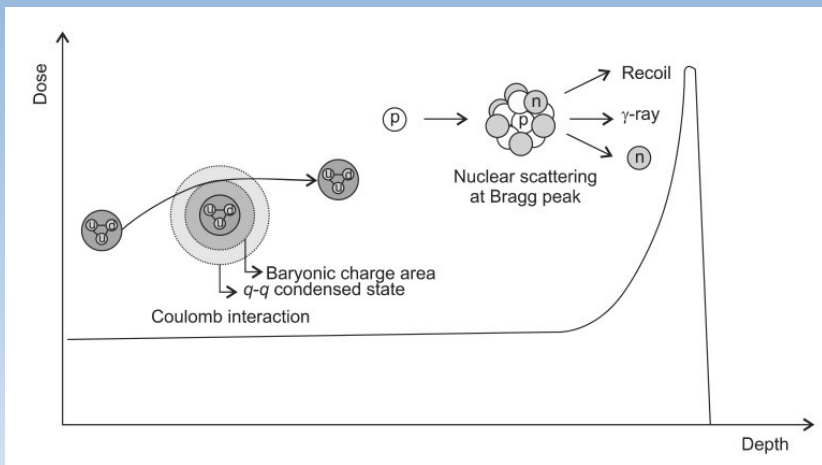
Motivation

- Cancer treatment: surgery, chemotherapy, radiotherapy, immunotherapy
- Radiotherapy: uses ionizing particles
- What kind of particles?
 - Photons
 - Protons
 - Heavy ions

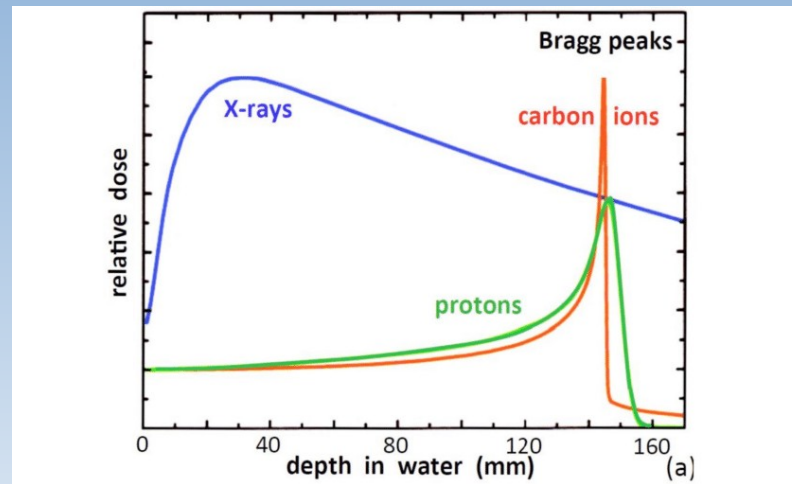


Layout figure of HIT Centre (Heidelberg)

Why is proton therapy so outstanding?

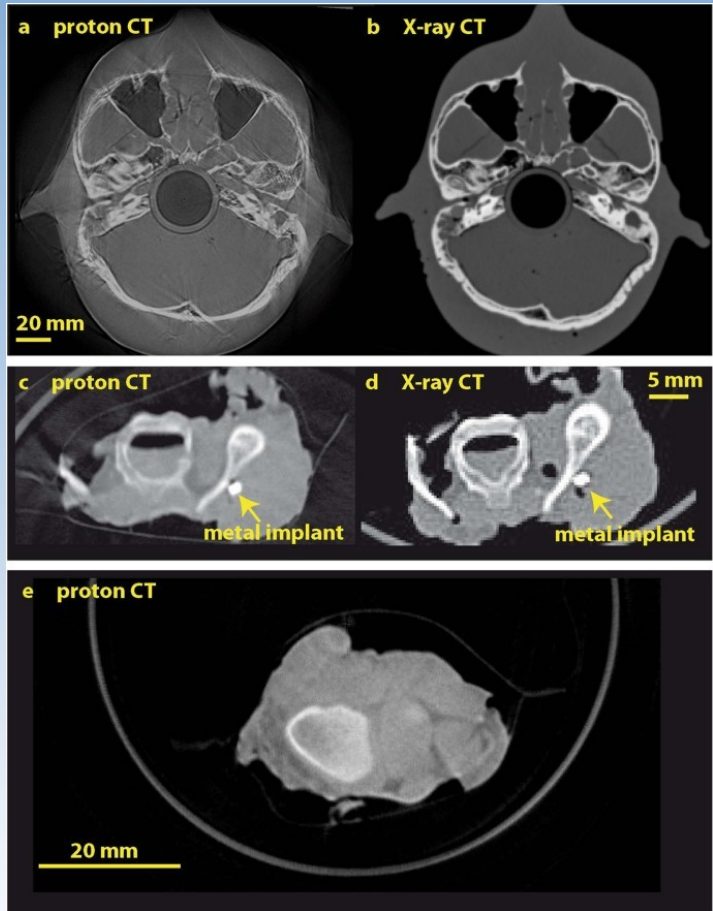


[Seo Hyun Park and Jin Oh Kang. Basics of particle therapy i: physics. Radiation oncology Journal, 29(3):135, 2011.]



[Ugo Amaldi, Manjit Dosanjh, Jacques Balosso, Jens Overgaard, and Brita Sørensen. A facility for tumour therapy and biomedical research in south-eastern europe. 09 2019.]

Problems with imaging – and the solution



X-ray CT vs. proton CT

- Today X-ray CT is used
- We need to know the range of the protons → Relative Stopping Power (RSP): how much does it slow down in a material compared to water
- Difference between the absorption of photons and the energy loss of protons → conversion is not accurate between Hounsfield units* and RSP
- Solution: let's do the imaging with protons! → proton CT

*The quantitative scale of X-ray absorption

The Bergen pCT Collaboration

Irradiating the phantom with high energy (~100 MeV) protons



Detector system senses the signals

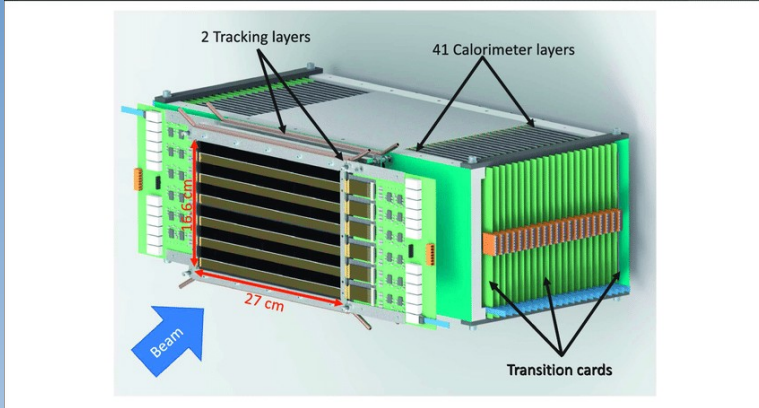


Processing the signals

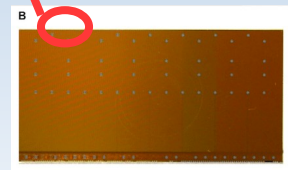
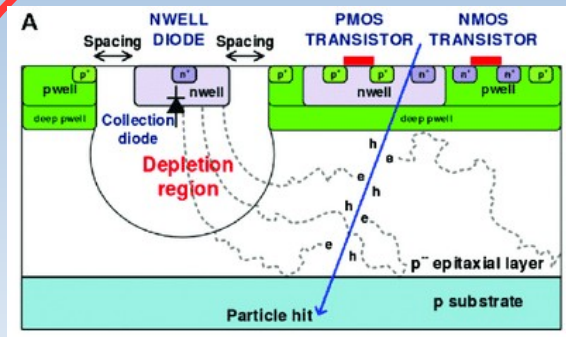


Reconstructing the image

- Based at the University of Bergen
- Goal: to build a proton CT based on the high-energy particle detectors used in the CERN ALICE collaboration (technology transfer)
- The detector system is based on the ALPIDE chip



The Bergen pCT

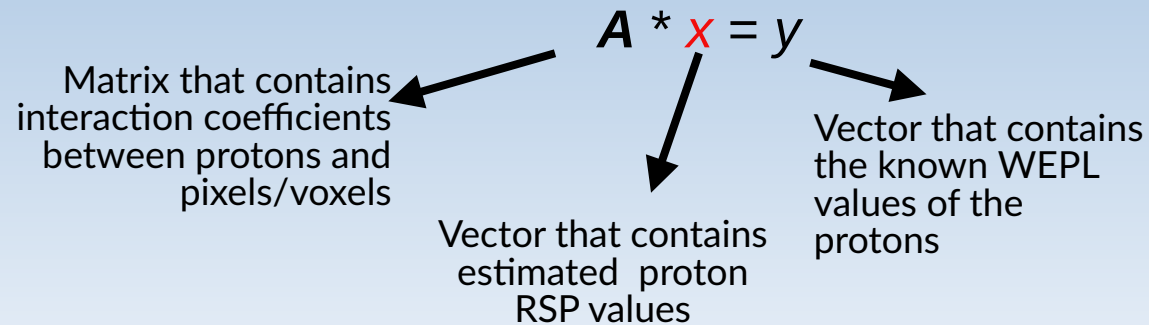
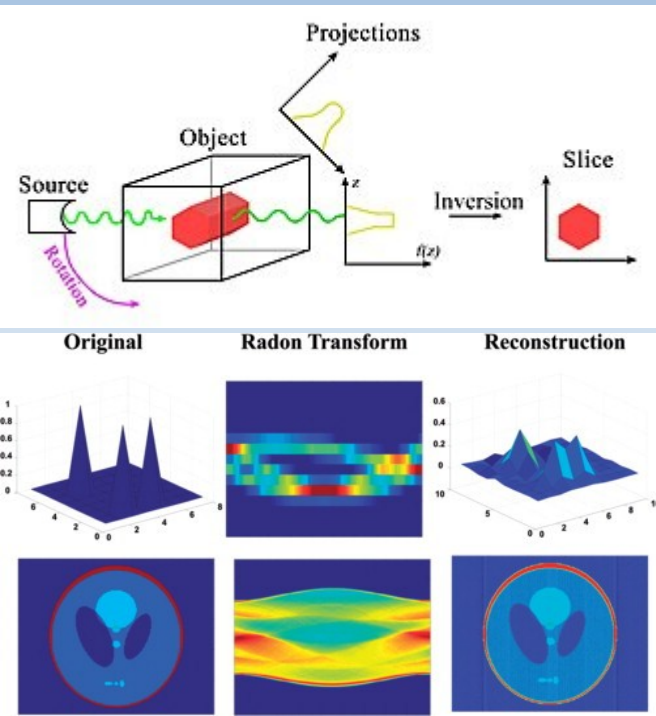


The cross-sectional image (A) and the photograph (B) of the ALPIDE chip

Image reconstruction techniques

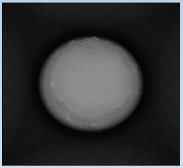
Integral transformations → Radon, Inverse Radon
→ Cannot be used for proton CT (due to nuclear scattering of protons)

Iterative reconstruction techniques
→ Model the problem as a linear equation system

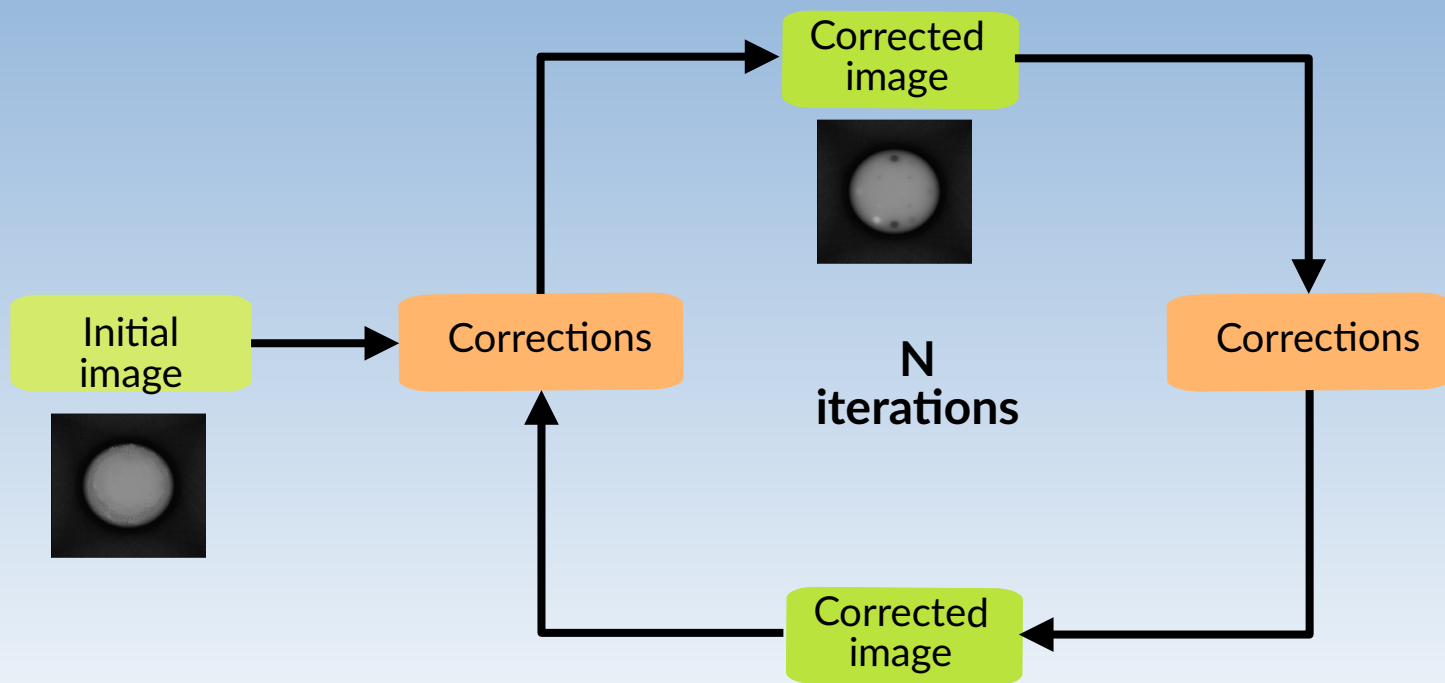


Iterative methods for image reconstruction

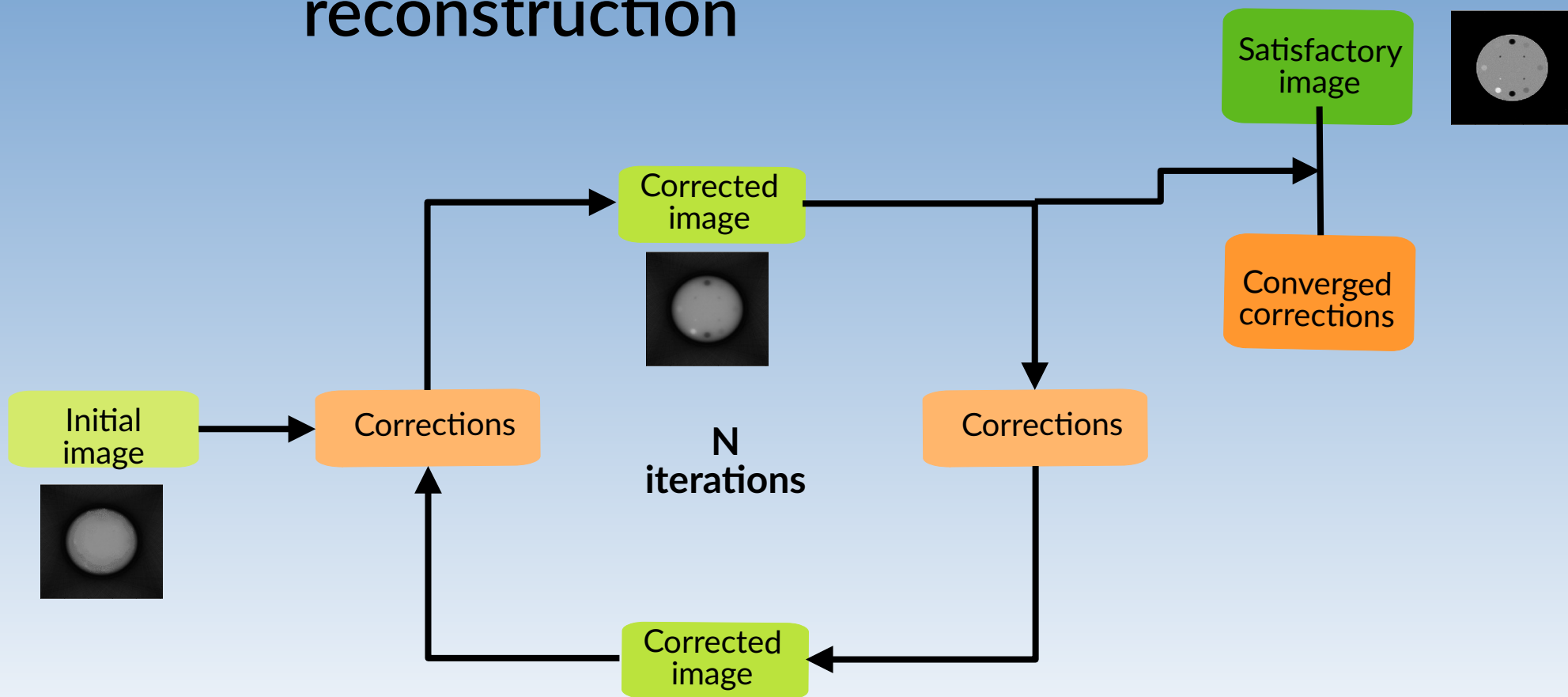
Initial image



Iterative methods for image reconstruction



Iterative methods for image reconstruction



The Richardson-Lucy algorithm

Number of iterations

Vector containing WEPL values

Matrix containing interaction coefficients between proton trajectories and voxels

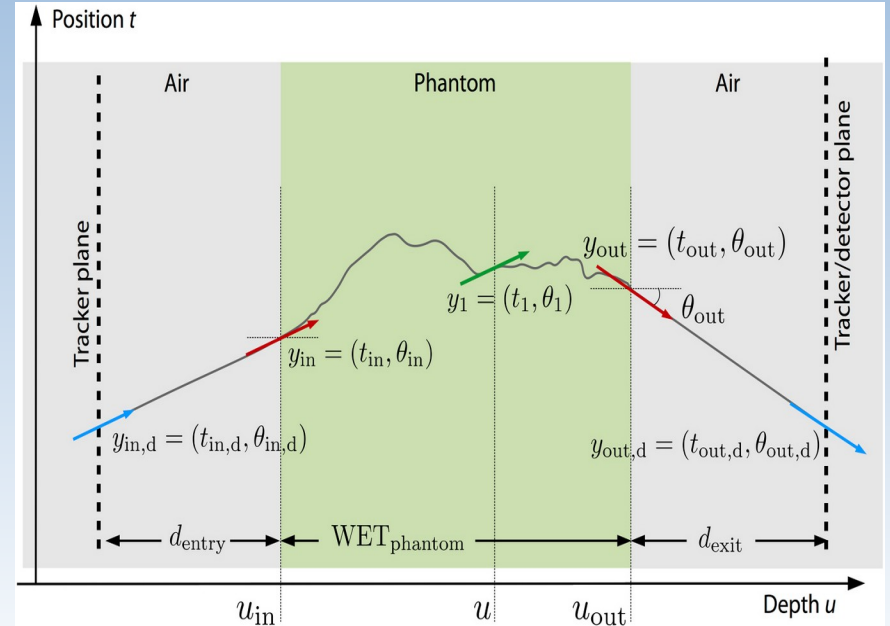
$$x_i^{k+1} = x_i^k \frac{1}{\sum_j A_{i,j}} \sum_j \frac{y_j}{\sum_1 A_{l,j} x_1^k} A_{i,j}$$

Vector containing RSP values

- Statistical iterative algorithm
- Maximum Likelihood - Expectation Maximization (ML-EM)
- Originally used in optics
- Input data: from detector or Monte Carlo
- MLP calculation
- RSP-distribution calculation

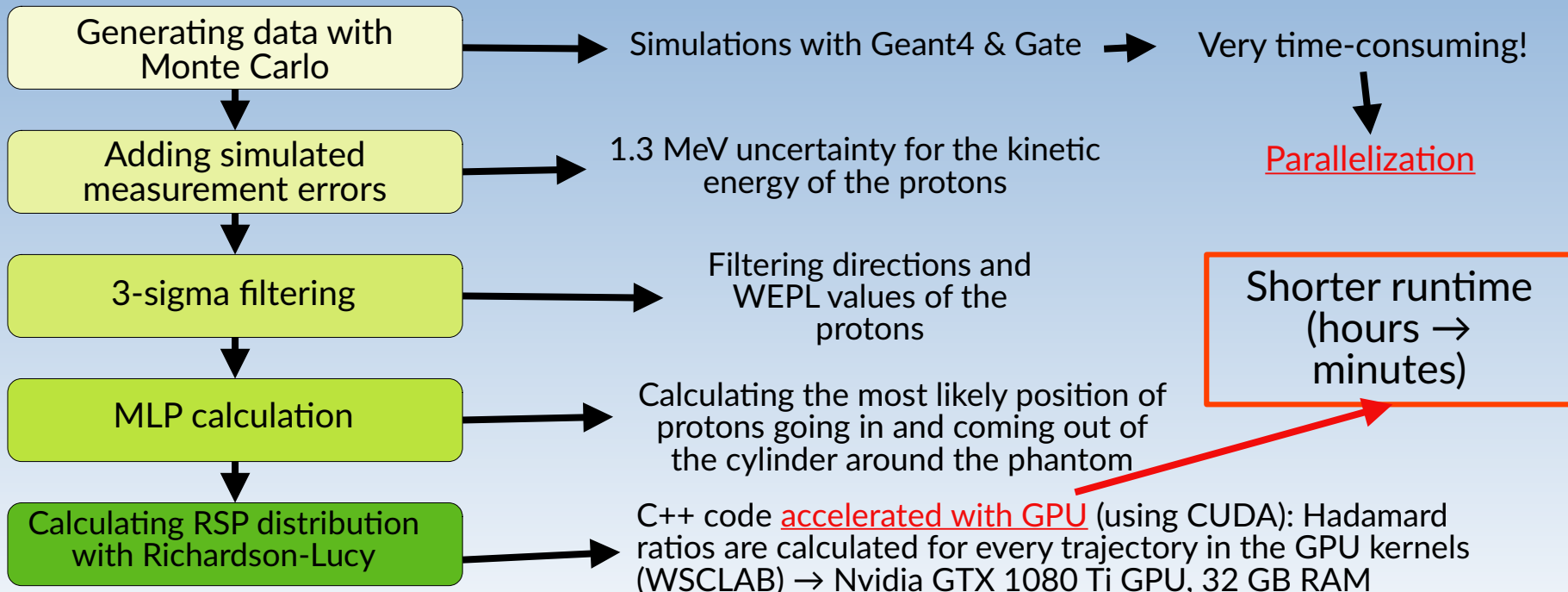
Very difficult technically (~millions of proton trajectories)

- Using GPU (CUDA)
- Goal: Finding optimization regarding the number of iterations and protons



Development of the framework

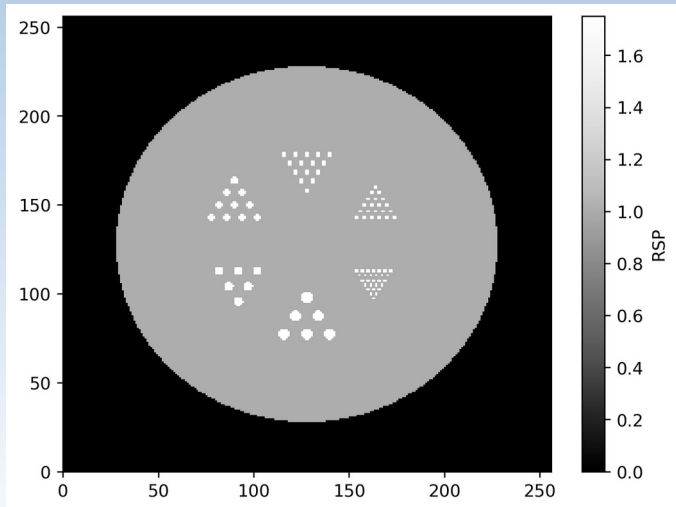
Steps of the framework



Evaluating the algorithm - phantoms

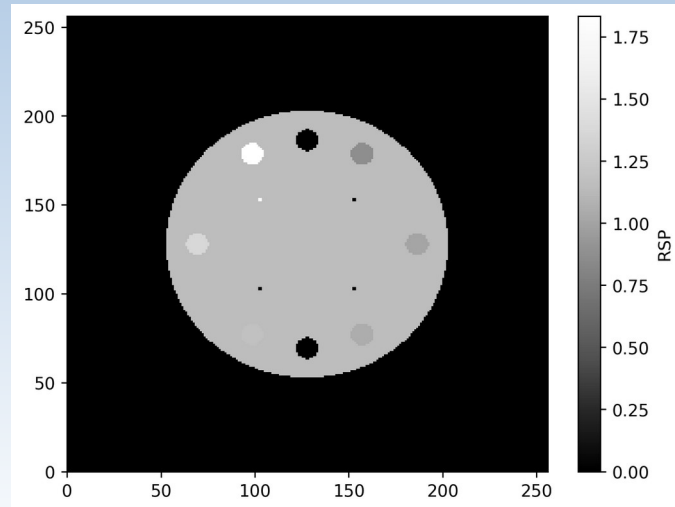
Derenzo phantom

- 200 mm diameter water cylinder with 6 sectors of 1.5-6 mm diameter aluminium rods
- Used for measuring spatial resolution

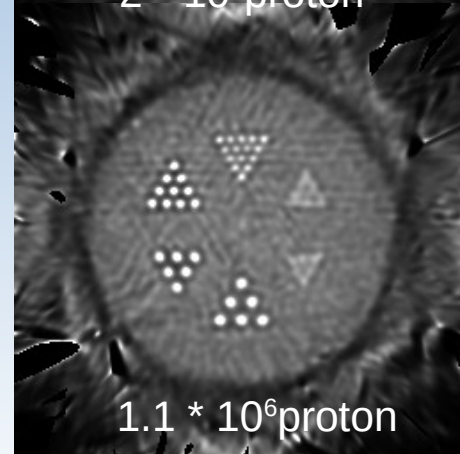
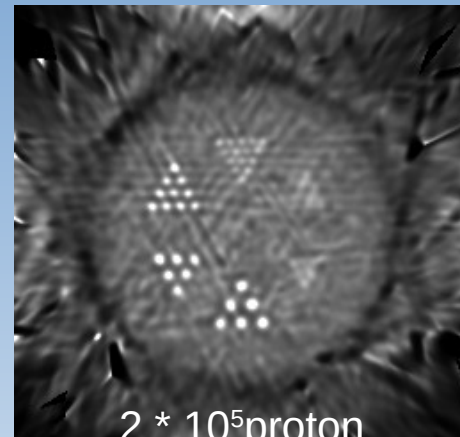
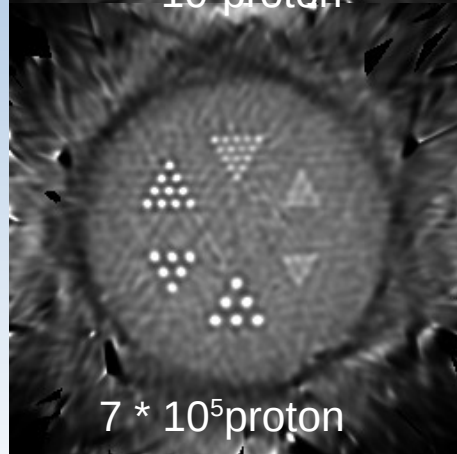
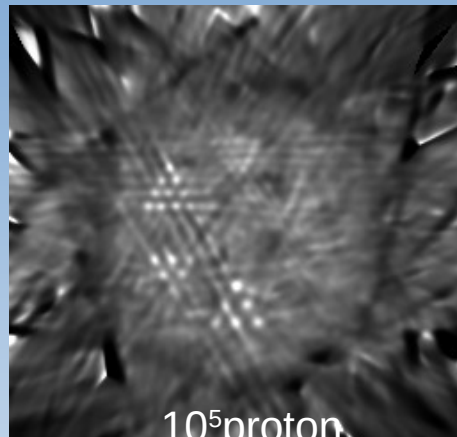
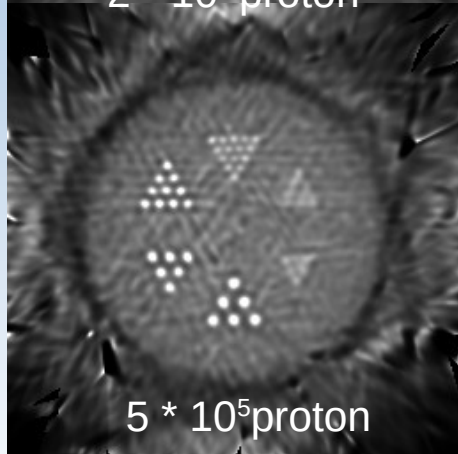
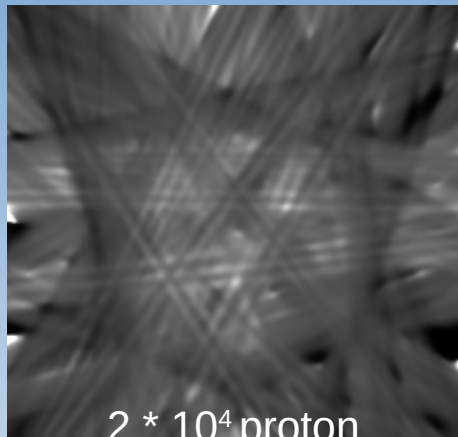


CTP404 phantom

- 150 mm diameter epoxy cylinder with 8 different material inserts with 12.2 mm diameter
- Used for measuring reconstruction accuracy for RSP

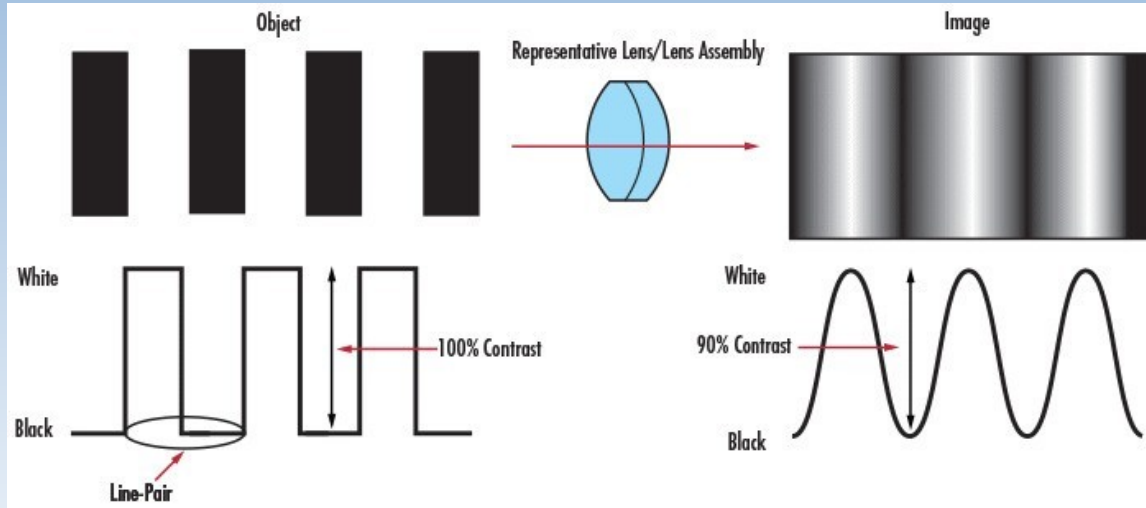


Spatial resolution with Derenzo phantom



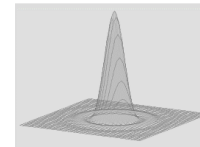
Spatial resolution with Derenzo phantom

Good measure for spatial resolution: Modulation Transfer Function → how well can we differentiate between two objects on an image



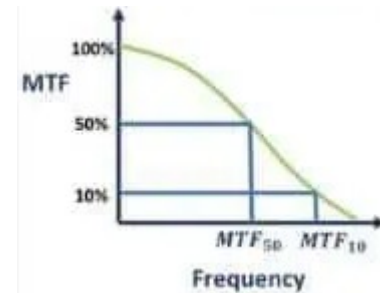
Modulation Transfer Function (MTF)

Image Space



Point Spread Function

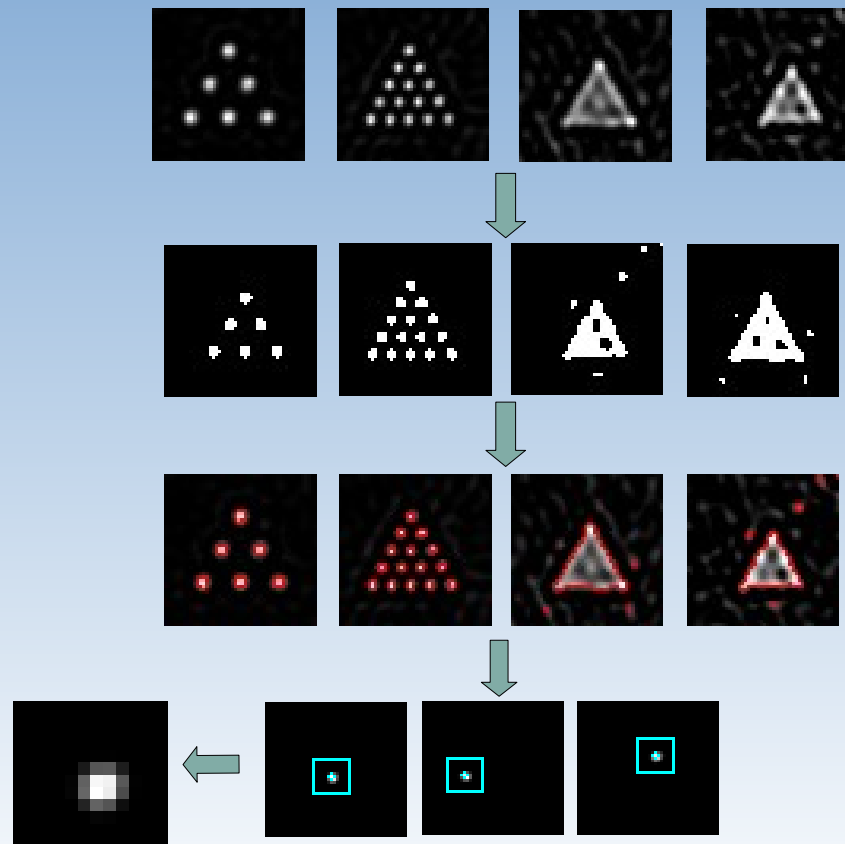
Fourier Transform



Spatial resolution with Derenzo phantom

Determination of the $MTF_{10\%}$

1. Get the (avg) PSF from each rod size (that is still distinguishable¹)
 - i. Subtract the mean background
 - ii. Rotate and cut the Area Of Interest (AOI)
 - iii. Try to search for the unique blobs
 - iv. Avg. the blobs
 - v. (Take the radial profile)
2. Get the MTF from the PSF
 - i. 2d Fourier transform of the PSF
 - ii. Radial profile
 - iii. Sigmoid fit
 - iv. Take the 10% value

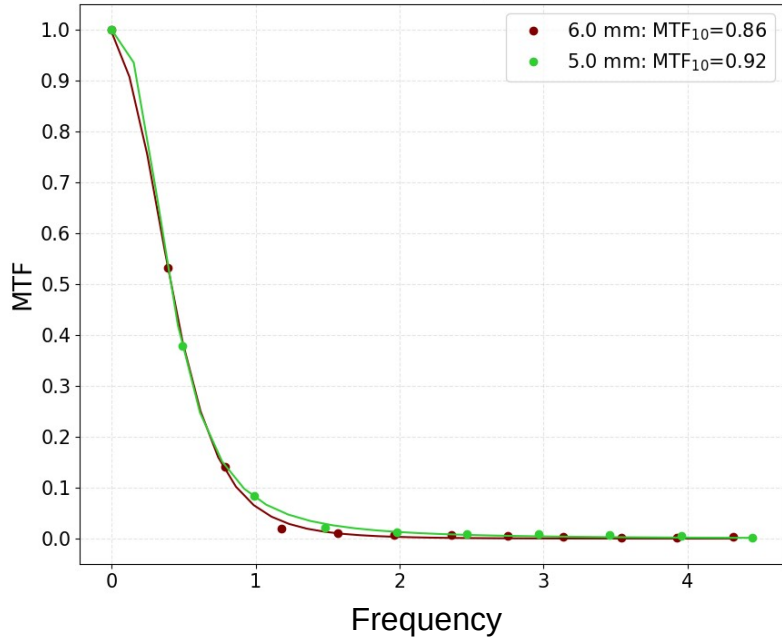


Zsófia Jólesz
GPU Day, 2024

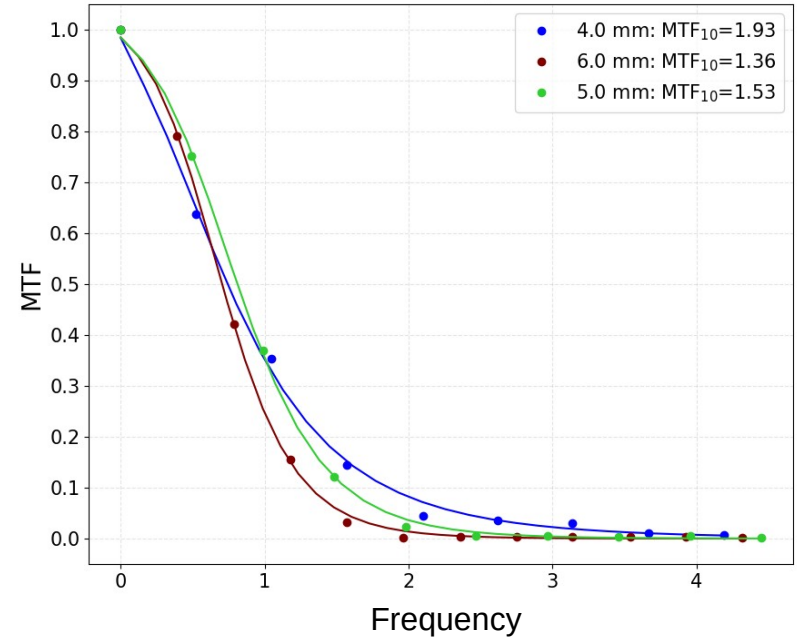
¹Hard limit determined by the pixel size, e.g. 256x256 geometry \rightarrow 1mm/px

Spatial resolution with Derenzo phantom

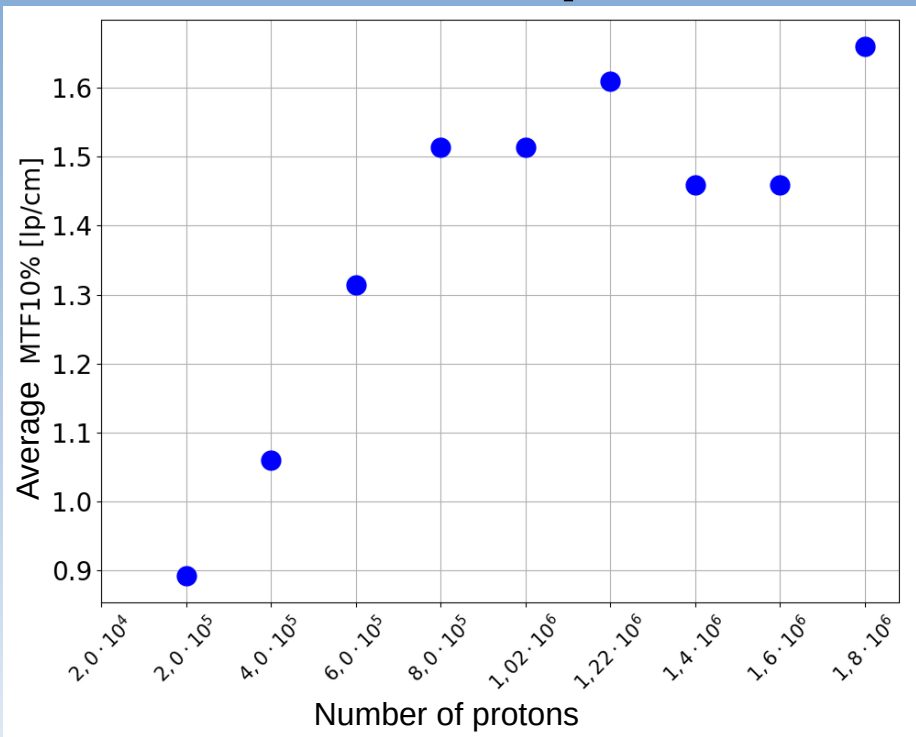
2.0×10^5 protons



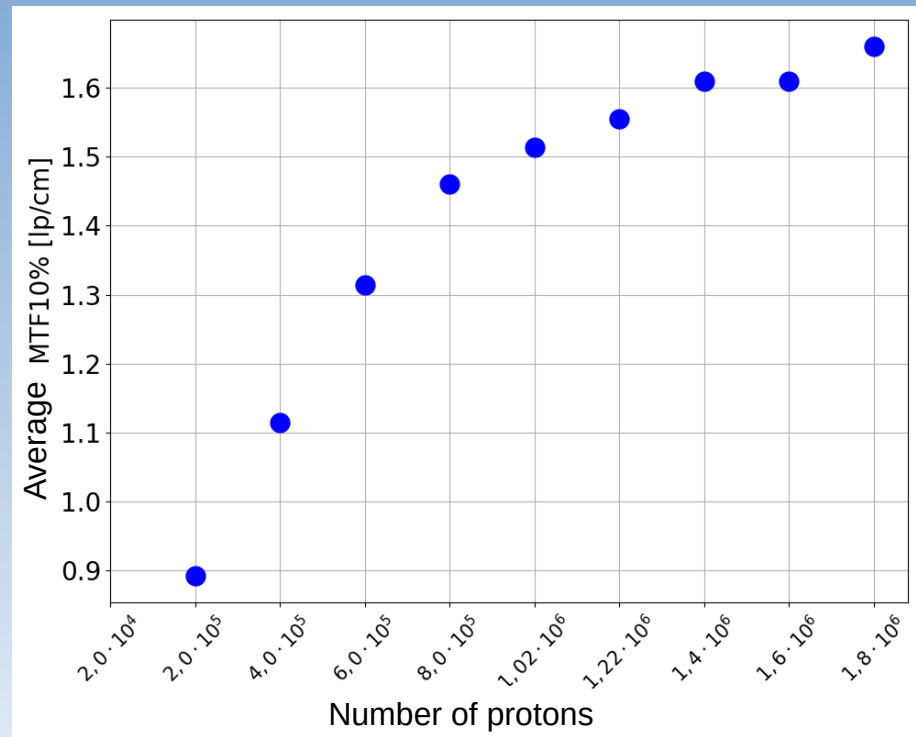
1.22×10^6 protons



Spatial resolution with Derenzo phantom



“Realistic” case

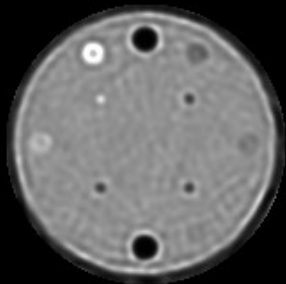


“Ideal” case
(no added error in energy)

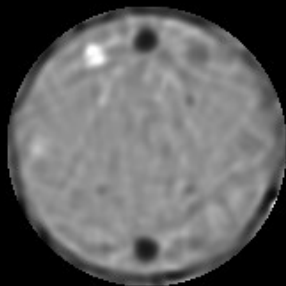
RSP reconstruction accuracy with CTP404 phantom



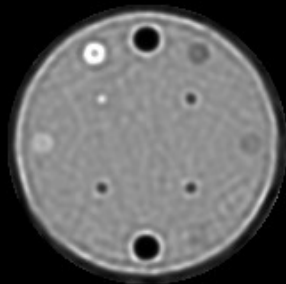
$2 * 10^4$ proton



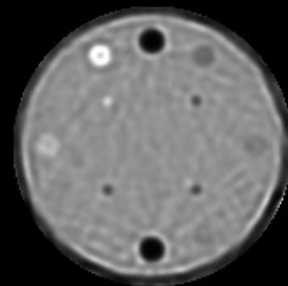
$5 * 10^5$ proton



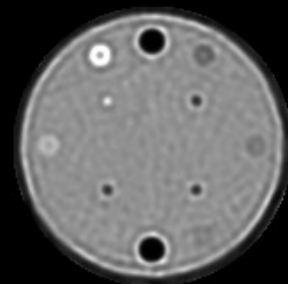
10^5 proton



$7 * 10^5$ proton

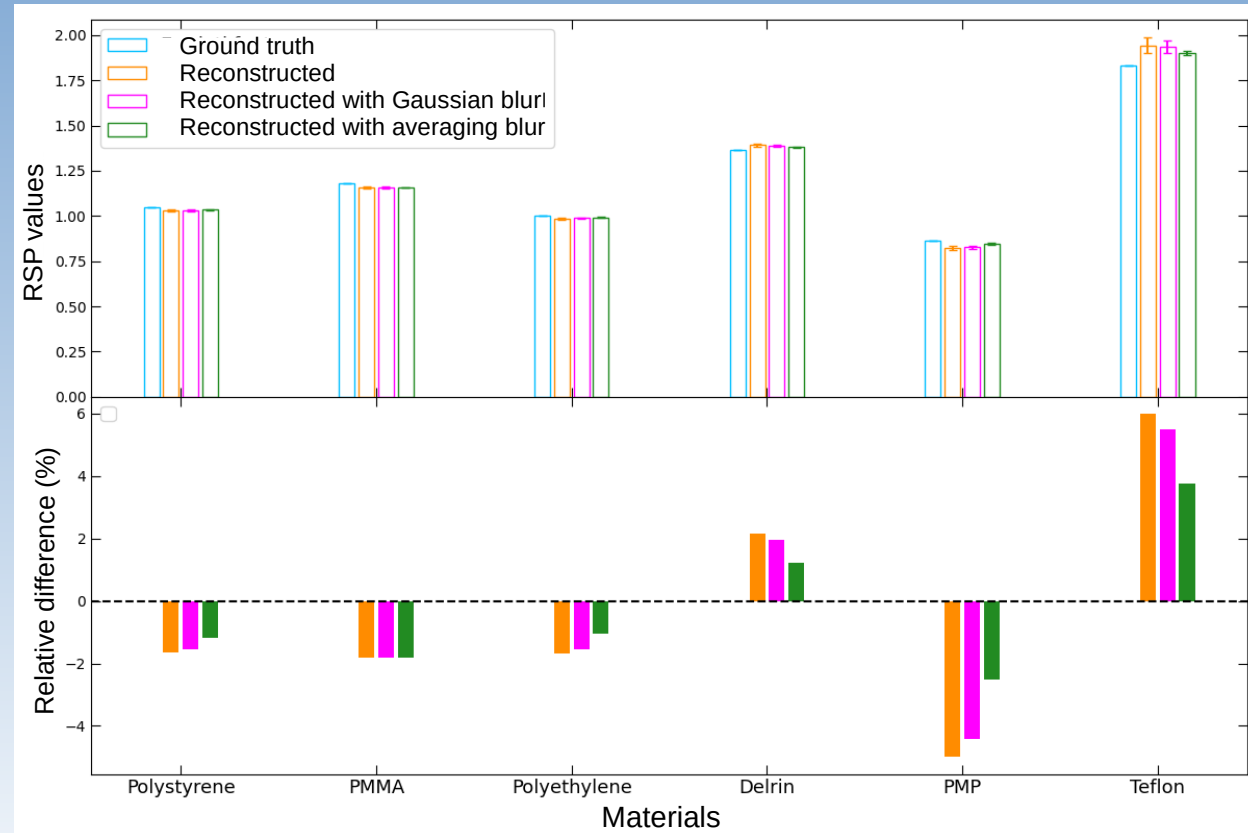
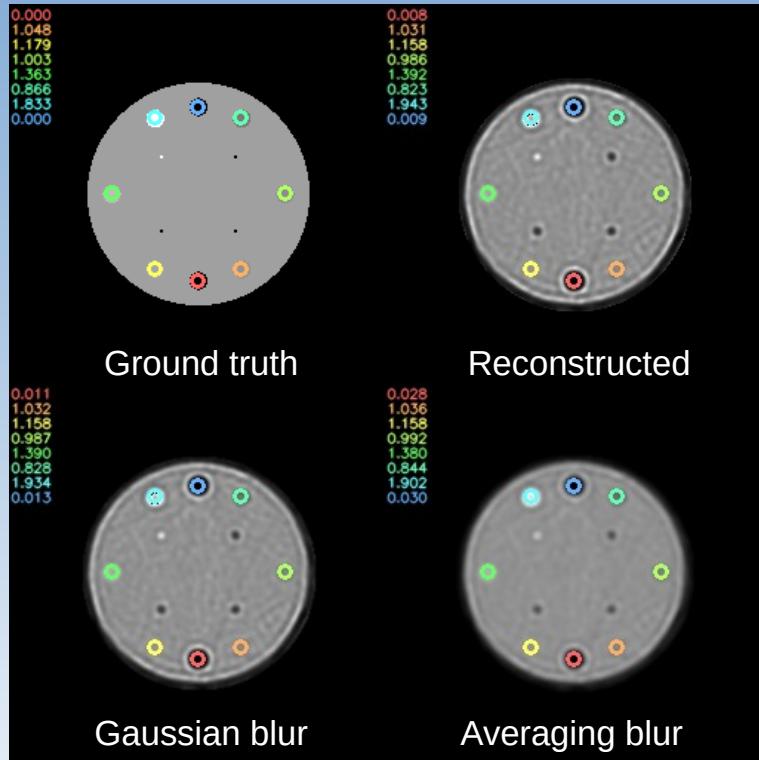


$2 * 10^5$ proton

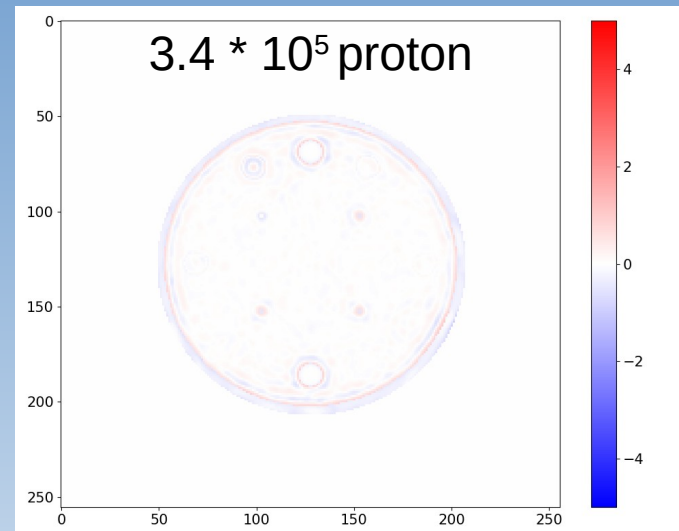
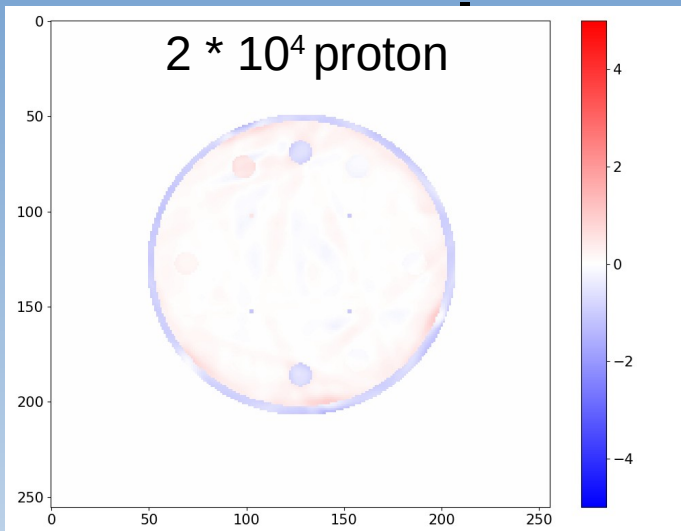


$1.1 * 10^6$ proton

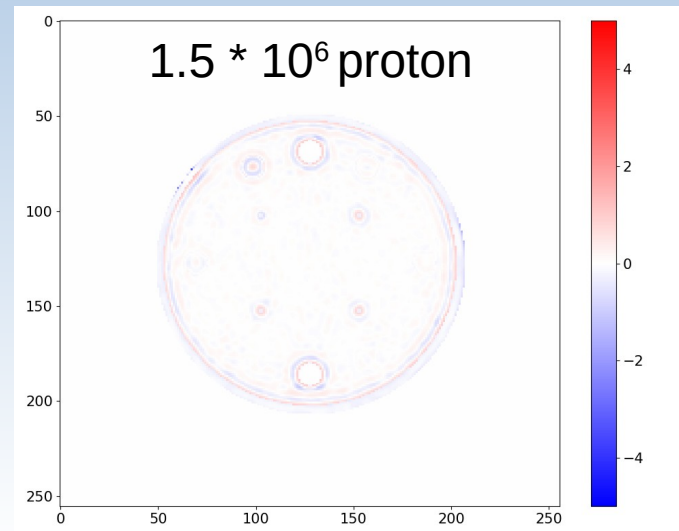
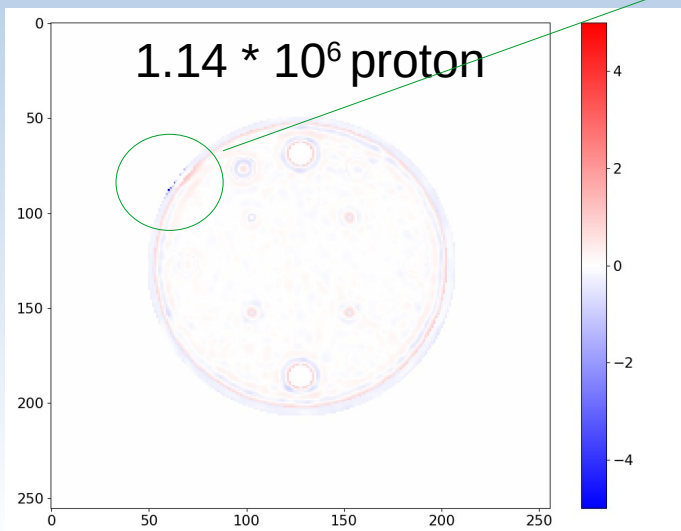
RSP reconstruction accuracy with CTP404 phantom



Differences between the RSP



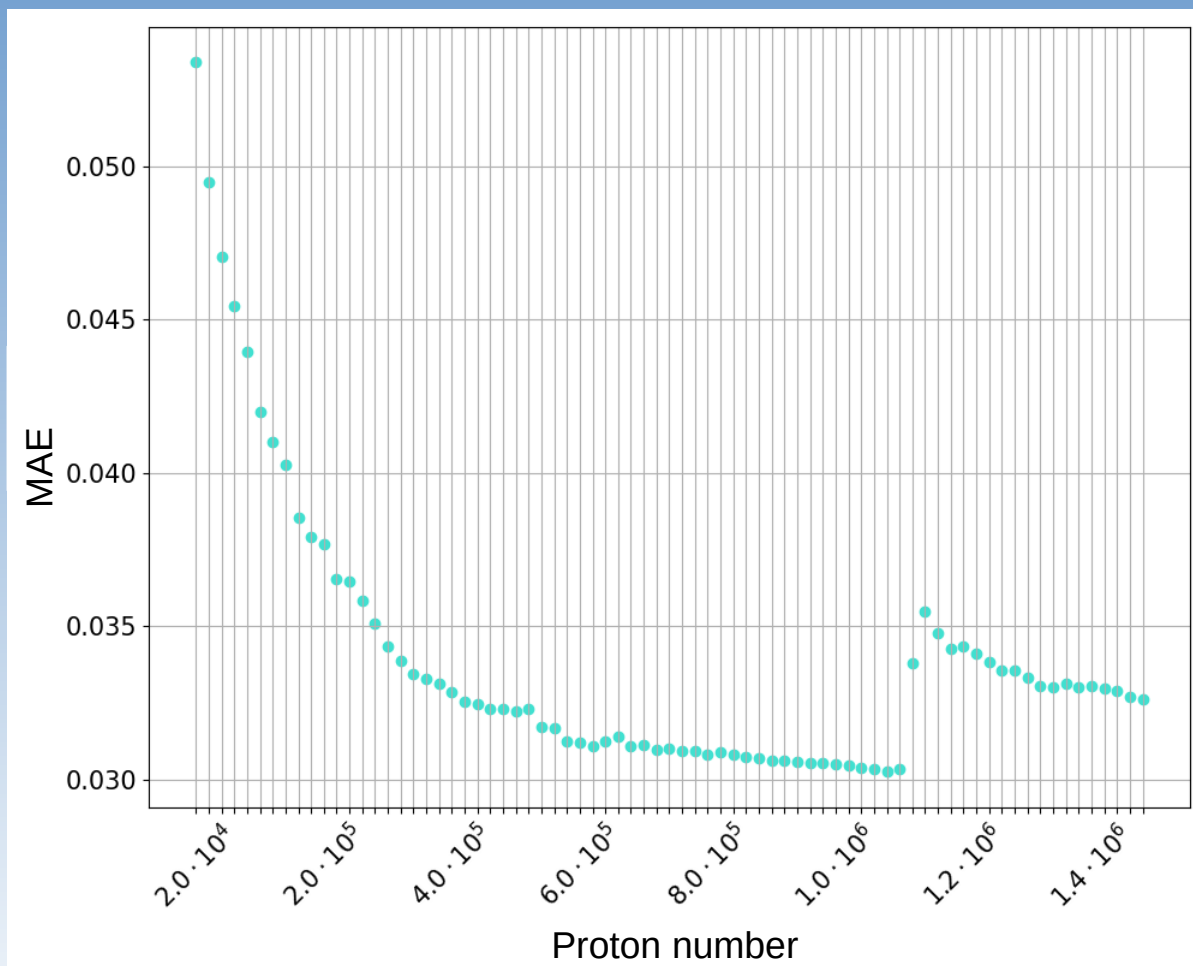
Some outlier pixels



Mean Absolute Error

Mean Absolute Error:
the average absolute
difference between
corresponding pixels

$$MAE = \frac{1}{mn} \sum_{i=1}^m \sum_{j=1}^n |\text{im1}(i, j) - \text{im2}(i, j)|$$



Comparison to other results in the literature

MTF10% values

	Ideal	Reference - ideal	Realistic	Reference - realistic
MTF10% [lp/cm]	0.9-1.7	2.6-3.7	0.9-1.7	2.4-3.0

Sølie et al., 2020

RSP reconstruction accuracy

- ~1% for Wang et al., 2010, runtime is more (Bayesian interference-based proton path probability map for MLP calculation)
- ~6% for our research, runtime is less (Cubic spline fitting for MLP calculation)

Zsófia Jólesz
GPU Day, 2024



Summary of achievements and future plans

- I have optimized a framework that utilises the Richardson-Lucy algorithm for pCT image reconstruction
- Tested the framework on two phantoms
- TDK Thesis → 3rd place

- Algorithm needs further developments for clinical usability → MLP calculation, shorter runtime, realistic phantoms, etc.
- MSc Thesis

Thank you for your attention!

My research was supported by the Hungarian National Research, Development and Innovation Office (NKFIH) grants under the contract numbers OTKA K135515 and 2021-4.1.2-NEMZ_KI-2004-00033.

Zsófia Jólesz
GPU Day, 2024